# **IRIA-ICRI** Guidelines and Recommendations

## (INDIAN RADIOLOGICAL AND IMAGING ASSOCIATION- INDIAN COLLEGE OF RADIOLOGY AND IMAGING )

## **Radiation and protocols in COVID 19 imaging**



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#### Prepared by AERB committee of Indian Radiological and Imaging Association

## **RADIATION— FRIEND OR FOE?**

- ✓ Natural emissions of ionizing radiation surround us and are found everywhere from the air we breathe, the food we eat, the ground we walk and the cosmic waves in our atmosphere. Such background radiation reaches a global average of ~2.4mSv/year and can further increase in certain higher radiation hotspots and high altitudes.
- ✓ While these remain beyond our control, artificially generated radiations in the form of diagnostic and therapeutic x-rays prove to be a bone of contention when it comes to the risk benefit analysis. There is no denying that radiation exposure is an issue of concern due to its genetic and carcinogenic effects.
- ✓ However, the benefits easily outweigh the risks when used under advisable limits and guidelines and unnecessary radio-phobia should be addressed by creating awareness.
- ✓ To put things into perspective;-- One time air travel from New Delhi to New York would expose one to ~0.08mSv of radiation, whereas 1 Chest X ray offers a radiation of mere <0.1mSv which with modern techniques can be reduced down to 0.02mSv. Moreover, no scientific studies have yet found an increased incidence of malignancies in frequent fliers or airline pilots.</p>

### **JUSTIFICATION:**

- ✓ All the investigations involving X rays must be clinically and radiologically justified.
  Only valid referrals after establishing a valid clinical indication should be accepted.
- Appropriate selection of imaging modality and protocol, best suited to answer the clinical question at that point of patient management must be suggested by responsible radiologist/ clinical colleague in consensus.
- ✓ Unnecessary repetitions must be discouraged or should be allowed only if the clinical status of the patient demands so, as pulmonary infections show a significant lag in radiological resolution as compared with clinical resolution.

### **OPTIMIZATION:**

The principal of **ALARA (as low as reasonably achievable)** must be practiced to optimize the individual radiation dosage. Adjusting the exposure settings to low kVp or mAs whenever possible, increasing the distance between X ray source and patient while decreasing the time of

exposure, collimating the X-ray beam to area of interest are a few ways to reduce radiation exposure.

CT has emerged to be the most often ordered imaging modality for diagnosing pulmonary diseases. With the technical advancements, we are now able to strike a balance between attaining adequate imaging quality and the radiation exposure by tapering the acquisition protocol according to the clinic-radiological indication.

For CT scanners, using all possible methods of dose reduction in the equipment should be consciously done. Many protocols are automated in current equipment. Most **dose reduction techniques** are based on decreasing kVp, mAs, rotation time and duration of scanning; limiting the area exposed to ROI, using higher pitch in volumetric scanning, using appropriate collimation, filters and kernels; as well as post processing techniques like edge enhancement, to gain maximum possible spatial information.

### **HRCT** protocols and radiation exposure

- Volumetric scanning in full inspiration has now superseded the conventional sequential technique. However, if availability is limited e.g. in peripheral centers, a sequential HRCT (1-2mm scans at 1.5-2 cm gaps) can be performed.
- Current suggested **HRCT technique** includes scanning in a supine position at end inspiration. It exposes the patient to ~**3-8mSv radiation** (kvp- 100-140, mAs- 120-200).
- Where repetitive imaging is required, **Low-Dose HRCT** should be recommended. It provides images of adequate diagnostic quality. The Radiation dose can be brought down to ~1-3mSV by modifications in kvp- 80-120 and mAs-<100.
- Ultra Low Dose HRCT, can aid in further dose reduction by using the mAs, thereby reducing the exposure to <1mSv. However, at present their role is limited to screening and surveillance scanning.

## Chest X-ray and their approximate effective radiation doses

Procedure	Average Effective	Range Reported in	Comparable to natural
	Dose(msv)	Literature	<b>Background Radiation</b>
			for
X-Ray Chest	0.1msv	0.05-0.24 msv	10 day

With **PA projection** the doses measured for the different devices were the following amorphous selenium system

- ✓ Routine Chest Xray 0.12+/-0.06mGy.
- $\checkmark$  CR system 0.3+/-0.05mGy
- ✓ DR system0.05+/-0.02mGy

#### Lateral projection amorphous Selenium system

- ✓ Routine chest X-Ray 0.40+/-0.13mGy
- $\checkmark$  CR system 0.9+/-0.17 mGy
- ✓ DR system0.21+/-0.15mGy

The use of Digital system allows significant reduction of the patient dose. In particularly the Direct Radiography system, based on a Csl/a-Si detector, administers the lowest patient dose

#### **Protection of Patient**

- 1.Using High peak kilovoltage and low miliampere-seconds
- 2.By Using lowest acceptable Grid ratio
- 3. Beam restriction
- 4. By using shield to unexposed area

5.Filtration

- 6.By using Fast speed Film and intensifying screens
- 7.Periodic maintenance of machine

# Ct scanners and their approximate effective radiation doses

СТ	Head		Orbit		PNS	
SCANNER						
	Average	effective	CTDIv mGy	Lens dose/		effective
	Ct Dose	dose m		effective		dose
	(CTDIv)	Sv		dose		
	mGy					
Single slice	GE CT/I -				toshiba - 19.67	
	CTDI –				mGy – CTDIw	
	40.1,				[2]	
	toshiba -					
	34.112					
4	55 mGy 3,					
	$32 \pm 4$					
6	17.7 - 20					
	mGy 9					
8	58.2mgy 4					
	GE					
16	64.96	1.2 +/-	104.45 +/-	98.58 +/-	15.9 - 26.9 14	0.73 - 0.94
	mGy 5,	0.5	6.7810	9.03		mSv14
				mGy10		
32	70.2 mGy					
	+/- 18					
	(CTDIv) 5					
64	75 mGy		58.34 +/-	53.57 +/-	57.7 +/- 34 mGy	$10.05 \pm 5.94$
	(CTDIv) 5		7.08 mGy10	10.0710	15	15
128	69.2 m Gy	$1.80 \pm$	Routine	Routine	15.9-21.4 14	0.6 - 1.4
	4	0.24	Head	head		mSv14
			protocol -	protocol –		(Effective
			47.55	4.9 mSv11		dose)
			mGy11			
			35.3 mGy	3.6 mSv		
			12	12		
			Low dose			
			protocol –	Low Dose		
			4.1 mGy11	protocol –		
				0.4 mSv11		
			1.0 - 2.6	0.1- 0.8		

			mGy12	mSv		
256	30.4 mGy6					
320						
CONE	2.49 mGy	1.2 mSv			2.9 – 5.7 mGy	0.27 mSv
BEAM	18				16(Carestream	(range 0.05-
					9300)	0.48 mSv
DECT	Siemens	Siemens			Siemens	
	Somotom -	somatom			Definition flash	
	71.8 mGv	1.46 -			– (low dose	
	7	1.67			protocol)2.2 –	
	,	1.07			5.3 mGy 17	
	Siemens					
	definition					
	flash - 67.9					
	mGv 4					
	Siemens					
	force dual					
	source -					
	192 slice:					
	47.3 4					
sequential /						
axial						
scanner [4]						
4			75.1mGy13	70.2 +/-		
				1.5		
				mGy13		
8	58.2 mGY		66.5mGv	56.6 +/-		
_			J	0.09 mGy		
16	57.7 to		85.8	71.5 +/-		
	62.8			2.4		
32	53.3 to					
	61.4					
64			Aquilion 64	Aquilion		
			_	64-		
			113.3	103.5+/-		
			Somatom	7.2		
			sensation	Somatom		
			cardiac 64 –	sensation		
			58.9	cardiac		
				64-		

			48.4 +/-	
			1.7	
HELICAL /				
MDCT [4]				
		65.1	66.7 +/-	
4			1.4	
8		50.9	45.6 +/-	
			0.7	
16	Somatom	59.6	48.7 +/-	
	emotion 16		0.9	
	- 39.6			
32	54.1 - 54.5			
64	58.3	Aquilion 64	Aquilion	
		-96	64-82.3	
		Somatom	+/- 7.3	
		sensation	Somatom	
		cardiac 64 –	sensation	
		51.5	cardiac	
			64- 42.6	
			+/- 09	
128	50.3 -			
	58.3			
dect - 128	53.4			
dect - 198	47.3			

#### References

1.Wallace, A.B., Einsiedel, P. and Stone, A., 2000. Comparative dosimetry and image quality for a GE CT/i single-slice helical and a GE lightspeed QX/i multi-slice helical CT scanner. *Australasian Physical and Engineering Sciences in Medicine*, *23*(4), pp.178-179.

2. Aliasgharzadeh, A., Mihandoost, E. and Mohseni, M., 2018. A survey of computed tomography dose index and dose length product level in usual computed tomography protocol. *Journal of cancer research and therapeutics*, *14*(3), p.549.

3.Garba, I., Engel-Hills, P., Davidson, F. and Tabari, A.M., 2015. Computed tomography dose index for head CT in northern Nigeria. *Radiation protection dosimetry*, *165*(1-4), pp.98-101.

4. American Association of Physicists in Medicine (AAPM), 2012. Adult routine head CT protocols.

5. Al Ewaidat, H., Zheng, X., Khader, Y., Abdelrahman, M., Mustafa Alhasan, M.K., Rawashdeh, M.A., Mousa, D.S.A. and Alawneh, K.Z.A., 2018. Assessment of radiation dose and image quality of multidetector computed tomography. *Iranian Journal of Radiology*, *15*(3).

6. Qing, L. and Ma, X., 2013. Application of 256-slice computed tomography with low radiation doses in neonates with hypoxic-ischemic encephalopathy. *Experimental and therapeutic medicine*, *6*(6), pp.1414-1416.

7. Tipnis, S., Thampy, R., Rumboldt, Z., Spampinato, M., Matheus, G. and Huda, W., 2016. Radiation intensity () and visibility of anatomical structures in head CT examinations. *Journal of applied clinical medical physics*, *17*(1), pp.293-300.

8. Lin, H.C., Lai, T.J., Tseng, H.C., Wang, C.H., Tseng, Y.L. and Chen, C.Y., 2019. Radiation doses with various body weights of phantoms in brain 128-slice MDCT examination. *Journal of radiation research*, *60*(4), pp.466-475.

9. Korir, G.K., Wambani, J.S., Korir, I.K., Tries, M.A. and Boen, P.K., 2016. National diagnostic reference level initiative for computed tomography examinations in Kenya. *Radiation protection dosimetry*, *168*(2), pp.242-252.

10. Tan, J.S.P., Tan, K.L., Lee, J.C.L., Wan, C.M., Leong, J.L. and Chan, L.L., 2009. Comparison of eye lens dose on neuroimaging protocols between 16-and 64-section multidetector CT: achieving the lowest possible dose. *American Journal of Neuroradiology*, *30*(2), pp.373-377.

11. Widmann, G., Juranek, D., Waldenberger, F., Schullian, P., Dennhardt, A., Hoermann, R., Steurer, M., Gassner, E.M. and Puelacher, W., 2017. Influence of ultra-low-dose and iterative reconstructions on the visualization of orbital soft tissues on maxillofacial CT. *American Journal of Neuroradiology*, *38*(8), pp.1630-1635.

12. Widmann, G., Dalla Torre, D., Hoermann, R., Schullian, P., Gassner, E.M., Bale, R. and Puelacher, W., 2015, March. Detection of midfacial and orbital fractures using ultralow dose CT and iterative reconstructions. European Congress of Radiology 2015.

13. Suzuki, S., Furui, S., Ishitake, T., Abe, T., Machida, H., Takei, R., Ibukuro, K., Watanabe, A., Kidouchi, T. and Nakano, Y., 2010. Lens exposure during brain scans using multidetector row CT scanners: methods for estimation of lens dose. *American Journal of Neuroradiology*, *31*(5), pp.822-826.

14. Varghese, B., Kandanga, I., Puthussery, P., Vijayan, D., Babu, S.H., Aneesh, M.K., Noufal, M., Binu, E.V., Babu, A.C., James, S.M. and Kumar, S., 2018. Radiation dose metrics in multidetector computed tomography examinations: A multicentre retrospective study from seven tertiary care hospitals in Kerala, South India. *The Indian journal of radiology & imaging*, *28*(2), p.250.

15. Mohamed, M.A.E., 2015. Estimates of effective dose in adult CT examinations.

16. Xu, J., Reh, D.D., Carey, J.P., Mahesh, M. and Siewerdsen, J.H., 2012. Technical assessment of a cone-beam CT scanner for otolaryngology imaging: image quality, dose, and technique protocols. *Medical physics*, *39*(8), pp.4932-4942.

17. Diklić, A., Zujić, P.V., Šegota, D., Debeljuh, D.D., Jurković, S., Brambilla, M. and Kalra, M.K., 2020. Optimization of paranasal sinus CT procedure: Ultra-low dose CT as a roadmap for pre-functional endoscopic sinus surgery. *Physica Medica*, *78*, pp.195-200.

18.Xu, J., Sisniega, A., Zbijewski, W., Dang, H., Stayman, J.W., Mow, M., Wang, X., Foos, D.H., Koliatsos, V.E., Aygun, N. and Siewerdsen, J.H., 2016. Technical assessment of a prototype cone-beam CT system for imaging of acute intracranial hemorrhage. *Medical physics*, *43*(10), pp.5745-5757.

19.Schulze, D., Heiland, M., Thurmann, H. and Adam, G., 2004. Radiation exposure during midfacial imaging using 4-and 16-slice computed tomography, cone beam computed tomography systems and conventional radiography. Dentomaxillofacial Radiology, 33(2), pp.83-86.

20 Prato A, et al. Radiol med 2005 PMID 16437042

- 21 Bacher k,et al.AJR Am J Roentogenol 2006
- 22 Clinical imaging byDennis M.Marchiori

23. Nardi C, Talamonti C, Pallotta S, Saletti P, Calistri L, Cordopatri C, Colagrande S. Head and neck effective dose and quantitative assessment of image quality: a study to compare cone beam CT and multislice spiral CT. Dentomaxillofacial Radiology. 2017 Oct;46(7):20170030.

24. Miracle AC, Mukherji SK. Conebeam CT of the head and neck, part 1: physical principles. American Journal of Neuroradiology. 2009 Jun 1;30(6):1088-95.

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